Deep Learning based Zero Watermarking for Authentication of Medical Records

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Abstract. The security of digital images is crucial since they often contain sensitive and confidential data. Unauthorized access to this data could result in severe penalties for the parties involved. Despite the availability of highly secure algorithms, security remains a significant concern due to the rapid emergence of new technologies that can breach it. Thus the proposed work implements a technique that makes the confidential data inaccessible to intruders. Hence fragile type of data hiding technique is used where even with the slightest tampering to the image by an attacker, the information i.e. watermark image is completely destroyed, hence preventing it from unauthorized access. Also, a hybrid transform including DTCWT and NSST is used to fuse two medical images to form a more sophisticated output image, which serves as the final watermark. Further, the zero watermarking model is implemented using the ResNet 50 DL model for more precise results and extraction of feature maps. Embedding the actual image in the carrier image could make the watermarking detectable especially when it is fragile, hence Zero Watermarking overcomes this also by virtual embedding. Moreover, the algorithm employs the avalanche effect of SHA512 for highly secure authentication, further strengthening the security of the system. Overall, the proposed method is an effective way to ensure the security of digital images with confidential data.

Keywords: Zero watermarking, Image Fusion, RDWT, Encryption, Medical images, Deep Learning.

1 Introduction

In today's digital age, the use of digital images has become ubiquitous in every sector of society, ranging from personal photography to medical imaging, from social media to e-commerce. With the increasing use of digital images, the need for their security has also become paramount. Digital images contain sensitive and confidential information, which if compromised, can lead to significant consequences such as identity theft, loss of personal privacy, and even financial losses. Therefore, it is imperative to ensure that digital images are adequately protected from unauthorized access, manipulation, and theft. This paper emphasizes the critical importance of ensuring the security of medical images, highlighting their vulnerability to unauthorized access and potential misuse. Various methods are employed for medical diagnosis, including ultrasonography, magnetic resonance imaging, positron emission tomography etc. Diagnostic images undergo an extensive array of processes, encompassing tasks such as feature selection, image denoising, and segmentation, and they are extensively archived and distributed [1].

One method of protecting digital images is through the use of watermarking. Various conventional techniques of watermarking have been employed by researchers to safeguard copyright in domains that are both fragile and robust.[2]. These techniques vary in their intended function and the level of security that they afford to digital data, as depicted in Figure 1.

Fragile watermarking is most effective in situations where digital media authentication is imperative. It employs a watermark as a digital signature, thereby validating the authenticity of the media and ensuring that it has not been altered. This feature makes it highly valuable in contexts of data authentication, where it is necessary to verify the genuineness of a document or image. [3]. On the contrary, robust watermarking is formulated to endure

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Fig. 1. Difference between Fragile and Robust Watermarking

typical signal processing attacks like compression, cropping, and filtering so that digital data still can be extracted. This makes it ideal for applications where the digital media needs to be distributed and shared widely, such as in the entertainment industry. However, the robustness of the watermark comes at the cost of reduced sensitivity, which means that it may not be able to detect small changes to the original digital media. Whereas, fragile watermarking is done in such a way that watermark data is completely destroyed after it encounters any change, it is harder for an attacker to modify or remove them without detection. Therefore, Fragile watermarking offers a higher level of security than robust watermarking. Therefore, this paper has opted for the fragile watermarking technique as the chosen approach for the necessary algorithm.

Over the recent years, researchers have extensively employed Zero watermarking, which can be thought of as "invisible watermarking." The usage of the term "zero" implies that the embedded watermark is crafted to remain unseen or imperceptible to human senses, such as sight or hearing, without causing any significant change in the original content's visual or auditory attributes. However, a significant portion of the research has centered around utilizing Zero watermarking as the robust algorithm. Hence, the authors undertook this study to explore the outcomes when the imperceptibility of Zero watermarking is integrated with fragile watermarking. The primary objective was to address the drawback of fragile watermarking, which is its susceptibility to detection compared to robust watermarking techniques.

In real-world scenarios, physicians often require multiple patient reports to make an accurate diagnosis. Taking this aspect into account, the present study has opted to consider that patients need to submit both their CT scan and MRI images. Addressing this concern, the paper introduces a fusion algorithm that can be described as a form of encryption and also a multi-factor authentication method.

The objective of this manuscript is to present a technique for securely transmitting digital images in a manner that ensures confidential information remains inaccessible to intruders and maintainting the authenticity of images.

2 Literature Survey

In recent years, with remarkable progress in deep learning techniques, they have also been extensively employed in safeguarding digital information. [4] paper proposed the first watermarking framework using CNN.It introduces a novel non-blind digital image watermarking method that utilizes the auto-encoder capability of CNNs. This approach generates positive and negative codebook images, which play a crucial role in embedding and extracting watermarks. But as their proposed method was completely non-blind, it lacks practicality in real world. DFT based Zero watermarking along with VGG19 and perceptual hashing was presented by authors in paper [5]. Though their framework was robust against various geometric attacks, but a CNN residual network with more deeper layers could give more accurate results than VGG19 which has 19 layers. Hence, within the algorithm presented in our paper, we opt for the utilization of Residual networks.

Authors of Ref. [6] proposed the method for Zero Watermarking with DCT and Residual DenseNet. Their proposed framework was robust against various geometric attacks. Further DWT-SVD-DCT based fragile watermarking was implemented in paper [7]. The authors developed a tamper-proof framework that could identify cropping and object insertion attacks. To enhance the framework's sensitivity and detect even minor alterations, an authentication code was generated and incorporated into the watermarked image using the QIM technique. The embedded code was extracted using the Gram-Schmidt process. However, it should be noted that the Gram-Schmidt process may result in information loss, which could erroneously detect an attack even if it did not occur. Further the paper has not analyzed results for many signal processing attacks.

Singh et al. [8] has put forward fragile watermarking technique using DCT-LSB method. While the paper's method is capable of accurately extracting the main content from a tampered image up to a 50% tampering rate, it is only effective in restoring against certain types of attacks. It cannot fully remove the watermark in cases of tampering, which is a crucial requirement for fragile watermarking as it must be highly responsive. Hence for making the algorithm highly sensitive and sensitive, hashing could also play the major role in authentiation. [9] paper completed the comparatively analysis of well known MD and SHA algorithms. Further concluded that for high security purpose SHA512 could serve the purpose because of its avalanche effect and longer length of string constructed.

Summing up the comprehensive review of existing literature, we deduced that Zero watermarking has predominantly been applied in robust methods. However, a drawback lies in the fact that while robust watermarking offers enhanced security, fragile watermarking surpasses it in terms of security measures. When it comes to employing watermarking techniques rooted in Deep Learning, a constant compromise between time complexity and result accuracy is unavoidable. As a result, our initial focus rests on the evaluation of

outcomes across different models, as detailed in subsequent sections. To bolster security, the integration of the SHA hashing algorithm stands out as a promising choice.

3 Proposed Methodology

This paper puts forth a fragile watermarking technique that is well-suited for binary images of a confidential nature (See Fig. 2). Until now, the majority of the existing fragile



Fig. 2. Framework of the proposed fragile watermarking model using image fusion

watermarking methods that embedded the watermark were easily detectable. However, the proposed approach employs zero watermarking, which doesn't embed the watermark directly but instead relies on the resemblances between the cover image and the watermark image. Unlike conventional zero watermarking methods, the proposed approach abstains from manual feature extraction and instead leverages the power of deep learning in conjunction with zero watermarking. We have devised a methodology that entails a 3 step process. Initially, fusion of two distinct watermarks is executed, resulting in the creation of a solitary watermark. Subsequently, the extraction of a feature map from the cover image is carried out. Finally, the zero watermark technique is implemented to accomplish the watermarking process. For the purpose of further enhancing security, hashing and scrambling of images is also carried out.

3.1 Watermark Generation using NSST-DTCWT transforms based Image Fusion

In this phase, DTCWT and NSST-based fusion of medical images is implemented to generate the watermark using two input images, CT' and MRI'. This image fusion algorithm uses two different rule sets to fuse the high and low-frequency coefficients of the input images. Parameter adaptive PCNN is used to fuse the high-frequency coefficients, while WSE and WSNML-based rules contribute to generating the fused low-frequency coefficients. The flowchart for generating the fused image as a mark carrier is shown in Fig.3.



Fig. 3. DTCWT-NSST based Image Fusion to generate final Watermark Image

To fuse the high-frequency coefficients, PA-PCNN-based fusion rules are adapted. PA-PCNN is a type of PCNN that works by monitoring the image processing performance and dynamically adjusting the parameters to optimize the results. This adaptation is performed through a feedback mechanism that adjusts the parameters based on the current state of the image processing. The parameters that are adapted in PA-PCNN include the coupling strength, the threshold and the pulse width.

PA-PCNNs can be used to preserve the relevant information from each image while suppressing the irrelevant information by automatically adjusting their parameters based on the input data. This enables the network to extract and preserve the most relevant features from each image, resulting in a fused image that contains more information than any of the individual images.

Further, the edge and contours of the input images are preserved by fusing the low-frequency coefficients of input images using a hybrid of WLE and WSEML. The activity level measure, WLE, is mathematically calculated as,

$$WLE_{ab}(x,y) = \sum_{i} \sum_{j} Wm'(i,j)H_{ab} \times (x+i,y+j)^2,$$
(1)

where $H_{ab}(x, y)$ denotes the high-frequency NSST coefficient at position (x, y) of direction b at layer a. Also, the Wm' is the weighted matrix which is defined as:

$$Wm' = \frac{1}{16} \begin{vmatrix} 1 & 2 & 1 \\ 2 & 4 & 2 \\ 1 & 2 & 1 \end{vmatrix}$$
(2)

Further, WSEML is used to extract the details of the input images using the following equation,

WSEML_{*a,b*}(*x, y*) =
$$\sum_{p=-rad}^{rad} \sum_{q=-rad}^{rad} (Wm'(p+rad+1, q+rad+1) \times EML_{a,b}(a+p, b+q))$$
 (3)

where, Wm' is the weighting matrix defined in eq. 2, and EML is defined as,

$$\begin{aligned} \operatorname{EML}_{img}(x,y) &= |2img(x,y) - img(x-1,y) - img(x+1,y)| \\ &+ |2img(x,y) - img(x,y-1) - img(x,y+1)| \\ &+ \frac{1}{\sqrt{2}} |2img(x,y) - img(x-1,y-1) - img(x+1,y+1)| \\ &+ \frac{1}{\sqrt{2}} |2img(x,y) - img(x-1,y+1) - img(x+1,y-1)| \end{aligned}$$

| Notation | Explanation | Notation | Explanation |
|----------------|--|-----------|---------------------------------------|
| CT MRI | Input images for multimodality | dtcwt_L1, | High and Low DTCWT |
| C_{1} , with | image fusion | dtcwt_H1 | coefficients of CT image |
| $nsst_L1$, | Low and high NSST | WLE1, | WLE and WSEML associated |
| $nsst_H1$ | coefficients of dtcwt_1 | WSEML1 | with dtcwt_H1 and dtcwt_H2 |
| $nsst_L$ | Fused low frequency NSST coefficient | nsst_H | Fused high frequency NSST coefficient |
| $dtcwt_H$ | Fused high frequency DTCWT coefficient | $dtcwt_L$ | Fused low frequency DTCWT coefficient |
| Fimg | Fused Image | cI | Cover Image |
| kov | Extraction Koy | fucedWI | fused Watermark Image |
| кеу | Extraction Rey | Tused W1 | after resizing |
| s WI | Watermark Image after | ResNet50 | Residual Network with |
| 5_ 11 1 | applying seed scrambling | | 50 layers |
| | contains weights of | | Feature Matrix of the |
| model | ResNet50 pre-trained on | FM | cover image predicted |
| | imagenet dataset | | using 'model' |
| DWT | Discrete Wavelet | SVD | Singular Value |
| | Transformation | | Decomposition |
| | Approximation, Vertical, | | Loft Middle and Bight |
| cA, cH, | Horizontal and Diagonal | 11 5 17 | singular matrices of ' cA ' |
| cV, cD | sub-bands of 'FM' on | u,s,v | on applying (SVD) |
| | applying DWT | | on applying 5 v D |
| h covor | Binary of the cover image | bin wat | Binary of the |
| D_cover | after hashing | Dill_wat | watermark image |
| CON | Binary of cover Image | S COV | Cover Image after |
| 00 | after adjusting its length | S_COV | applying seed scrambling |

 Table 1. Details of notations used in this article

As shown in Algorithm 1, two input images, 'CT' and 'MRI', are decomposed into high-pass and low-pass components using DTCWT transform. The resultant high-pass components, 'dtcwt_H1' and 'dtcwt_H2', are merged using a parameter adaptive PCNN (PAPCNN)-based fusion scheme, resulting in 'dtcwt_H'. Further, NSST is applied to the low-pass DTCWT coefficients. The resultant high-band NSST coefficients are again fused based on fusion rules using PAPCNN. The energy preserving and detail extracting issues are addressed by fusing the low-band NSST coefficients using WLE and WSEML-based fusion rules, generating the fused low-band NSST component, 'nsst_L'. Inverse NSST is then applied to form the fused low-pass DTCWT coefficients, 'dtcwt_L'. Finally, inverse DTCWT is applied to obtain the fused image, 'Fimg', which is treated as watermark image in the later sections.

3.2 Extraction of Feature maps

The extraction of feature maps is a crucial process that necessitates meticulous attention and consideration to guarantee the precision, dependability, and utility of the resulting

| Α | lgorithm 1: Algorithm of DTCWT-NSST based medical image fusion |
|-----------|---|
| | Input : CT, MRI |
| | Output: Fing |
| | <pre>// Phase 1: Transforming input images using DTCWT</pre> |
| 1 | $dtcwt_L1, dtcwt_H1 \leftarrow DTCWT(CT);$ |
| 2 | $dtcwt_L2, dtcwt_H2 \leftarrow DTCWT(MRI);$ |
| | <pre>// Phase 2: Transforming low-frequency sub-band using NSST</pre> |
| 3 | $nsst_L1, nsst_H1 \leftarrow NSST(dtcwt_L1);$ |
| 4 | $nsst_L2, nsst_H2 \leftarrow NSST(dtcwt_L2);$ |
| | <pre>// Phase 3: Fusion of low-frequency NSST coefficients</pre> |
| 5 | $WLE1 \leftarrow WLE_Calculation(nsst_L1);$ |
| 6 | $WLE2 \leftarrow WLE_Calculation(nsst_L2);$ |
| 7 | $WSEML1 \leftarrow WSEML_Calculation(nsst_L1);$ |
| 8 | $WSEML2 \leftarrow WSEML_Calculation(nsst_L2);$ |
| 9 | $map \leftarrow (WLE1 \times WSEML1 \ge WLE * WSEML2);$ |
| 10 | $nsst_L \leftarrow map. * nsst_L1 + map. * nsst_L2;$ |
| | <pre>// Phase 4: Fusion of high-frequency NSST coefficients</pre> |
| 11 | $nsst_P1 \leftarrow PA_PCNN(nsst_H1);$ |
| 12 | $nsst_P2 \leftarrow PA_PCNN(nsst_H2);$ |
| 13 | $map \leftarrow (nsst_P1 \ge nsst_P2);$ |
| 14 | $nsst_H \leftarrow map. * nsst_P1 + map. * nsst_P2;$ |
| | <pre>// Phase 5: Applying inverse NSST decomposition</pre> |
| 15 | $dtcwt_L \leftarrow Inverse_NSST(nsst_L, nsst_H);$ |
| | <pre>// Phase 6: Fusion of high-frequency DTCWT coefficients</pre> |
| 16 | $dtcwt_P1 \leftarrow PA_PCNN(dtcwt_H1);$ |
| 17 | $dtcwt_P2 \leftarrow PA_PCNN(dtcwt_H2);$ |
| 18 | $map \leftarrow (dtcwt_P1 >= dtcwt_P2);$ |
| 19 | $dtcwt_H \leftarrow map. * dtcwt_P1 + map. * dtcwt_P2;$ |
| | <pre>// Phase 7: Applying inverse DTCWT decomposition</pre> |
| 20 | $Fimg \leftarrow Inverse_DTCWT(dtcwt_L, dtcwt_H);$ |
| 21 | return Fimg |

features in required applications.

The approach taken in this paper involves the utilization of ResNet50 whose building block is shown in fig.4, a convolutional neural network (CNN) with a significant depth of 50 layers. The depth of the network is crucial for neural networks, but deeper networks are



Fig. 4. Residual learning: a building block[10]

more difficult to train. The configuration of ResNet50 enables the instruction of networks and permits them to be considerably more profound, resulting in augmented proficiency in various tasks. ResNet50 surpasses their simple equivalents in depth, and furthermore,

the quantity of weights in such networks is significantly lower. [11].

When a 512x512 cover Image 'cI' is fed through a modified ResNet50 model, the last convolutional layer produces a feature map with a spatial size of 16x16 and 2048 channels. Each channel in the feature map represents a specific learned feature of the input image. To obtain a final feature matrix, the individual feature maps are added element-wise to produce a single feature map. This final feature map preserves the spatial structure of the input image and contains information about the learned features across all channels. This feature map is used for further processing.

In ResNet50, the feature maps are extracted through a series of convolutional layers that are arranged in blocks. Each block consists of multiple layers, including convolutional layers, batch normalization layers, and activation layers. The output of each block is then passed through a shortcut connection that allows the gradient to flow more easily during training. In proposed method, we have used pre-trained model of ResNet50 on Imagenet Dataset.

3.3 Zero Watermarking

As described in[12], Zero watermarking essentially performs a virtual embedding process, where the key for generating a watermark is generated by analyzing the similarities between the attributes of the cover image and the watermark image. This key can then be used to produce an identical watermark from the cover image.

Method used for Zero Watermarking is described in Algorithm 2. The fused image 'Fing'

```
Algorithm 2: Watermarking
   Input : Fimg, cI
   Output: key
   // Phase 1: Resizing of input images
        fusedWI \leftarrow resize(Fing, (256, 256));
 1
        cI \leftarrow resize(cI, (512, 512));
 2
   // Phase 2: Scrambling of fusedWI
       s_WI \leftarrow seed\_scramble(fusedWI);
 3
   // Phase 3: Feature Map Extraction
        model \leftarrow ResNet50(weights = `magenet');
 4
        cI \leftarrow resnet50.preprocess\_input(cI);
 5
        FM \leftarrow model.predict(cI);
 6
   // Phase 4: Apply DWT and SVD
        [cA, cH, cV, cD] \leftarrow dwt(FM);
 7
        [u, s, v] \leftarrow svd(cA);
 8
   // Phase 5: Hashing Cover Image
        b\_cover \leftarrow SHA512(s);
 9
   // Phase 6: Adjusting length of binary of cover image
        bin\_wat \leftarrow matrix\_to\_binary(s\_WI);
10
        cov \leftarrow add\_trailing\_zeros(b\_cover, bin\_wat);
11
   // Phase 7: Scrambling binary of cover image
        s\_cov \leftarrow seed\_scramble(cov);
12
   // Phase 8: Key Generation
        key \leftarrow XOR(s\_cov, bin\_wat);
13
      return key
14
```

obtained after combining 'CT' and 'MRI' in Algorithm 1 serves as the watermark image. It is used as input along with the cover image 'cI'. After resizing, 'Fimg' is scrambled using Computer Science & Information Technology (CS & IT) 137 a seed scrambling algorithm. A feature map is extracted from 'cI' using the ResNet50 DL model that has been pre-trained on the imagenet dataset. This feature map 'FM' is then divided into frequency subbands with DWT, and the 'LL' subband is subject to SVD decomposition. The resulting 's' singular value matrix is hashed with the SHA512 algorithm. Both the scrambled watermark image ' s_-WI ' and the hashed string ' b_-cover ' are converted to binary form. To account for differences in size between the two binary outputs, a string of trailing zeroes is added to ' b_-cover ', and the same scrambling algorithm as previously mentioned is applied. The XOR operation is then performed on ' bin_-wat ' and ' s_-cov ' to generate the extraction key 'key'.

4 Results and Analysis

This part of the analysis thoroughly analyzes the suggested technique, beginning with experimental configurations and progressing to performance evaluation with varied cover images and fusion images. The comparative study of the proposed technique is offered at the end.

The trial begins initially by taking a brain MRI picture sized 512×512 as the cover object and the covert data is taken as a CT Scan image sized 256×256 . The implementation is done on MATLAB R2021b using system with the following configuration, Intel Xeon(R) Gold processor with 256GB RAM. The performance metrics used for assessing the projected technique are listed as (PSNR), SSIM, and NC. The evaluation parameters of Fusion method quantifies how accurately the fused image conveys the original images content. Some common fusion parameters are MI, QABF, SSIM, SF, and STD [13–15]. Visual output for 6 sample input output pairs are shown in table 2.

| Pair No. | Image 1 | Image 2 | Fused Im- age |
|----------|---------|-----------------|------------------|
| Pair 1 | | S | |
| Pair 2 | | | Ô |
| Pair 3 | | (\mathcal{O}) | |
| Pair 4 | | | |
| Pair 5 | Si | | |
| Pair 6 | | | |

Table 2. Sample of images used for evaluating Dtcwt-Nsst based multi-modality image fusion

The objective evaluation of the proposed DTCWT-NSST based fusion method, when implemented on 50 pairs of medical images [16], is referred to in Table 3. Average scores

| Pair | Entropy | MI | QABF | FMI | NABF | SSIM | SF | STD | PSNR1 | PSNR2 |
|------------------------|---------|---------|--------|--------|--------|--------|--------|---------|---------|---------|
| Pair 1 | 1.7126 | 3.4252 | 0.1937 | 0.8895 | 0.0373 | 0.0932 | 4.2698 | 36.2066 | 59.8872 | 66.1457 |
| Pair 2 | 6.7562 | 13.5125 | 0.4596 | 0.8789 | 0.2290 | 0.4766 | 6.0882 | 54.8540 | 70.0475 | 59.1952 |
| Pair 3 | 2.9538 | 5.9075 | 0.3288 | 0.8700 | 0.0452 | 0.6626 | 5.4185 | 84.7166 | 65.8571 | 59.2004 |
| Pair 4 | 4.4879 | 8.9757 | 0.2748 | 0.8929 | 0.0731 | 0.8234 | 4.5951 | 57.0351 | 70.13 | 65.7703 |
| Pair 5 | 4.8135 | 9.6269 | 0.3957 | 0.8821 | 0.0769 | 0.6659 | 5.8501 | 83.0159 | 65.8074 | 59.3964 |
| Pair 6 | 4.3270 | 8.6540 | 0.3049 | 0.8672 | 0.0666 | 0.5857 | 6.5350 | 80.7836 | 65.4172 | 58.8764 |
| Average of 50 pairs | 3.8406 | 7.6811 | 0.2906 | 0.8771 | 0.0419 | 0.6653 | 4.9579 | 79.5419 | 67.1835 | 59.9599 |

Table 3. Evaluation of proposed image fusion method on 50 pair of medical images

of QABF, FMI, SSIM, SF, and STD for 50 pairs are 0.2906, 0.8771, 0.6653, 4.9579 and 79.5419, respectively. These results verify the satisfactory performance of the multi-modality fusion method for healthcare images.

Table 4 displays a range of standard images employed for analyzing outcomes, while a medical image data-set of over 250 MRI images is also utilized for the same objective.

| I1 | I3 | I5 | I7 | I9 | I11 |
|----|----|---------------------|----|-----|----------------------------------|
| | Ø | | | | |
| I2 | I4 | I6 | I8 | I10 | I12 |
| | | 443-45 ⁷ | | | Average of 250+ MRI Images |

Table 4. Standard Images

The proposed method is being tested against various geometric and signal processing attacks, as illustrated in table 5. NC value is calculated original watermark and extracted

Table 5. Attacks performed

| Symbol | Attack Names |
|--------|----------------------|
| A1 | Average filtering |
| A2 | Cropping Attacks |
| A3 | Gaussian filter |
| A4 | JPEG compression |
| A5 | Median Filter Attack |
| A6 | Rotation Attack |
| A7 | Salt & Pepper Noise |
| A8 | Scaling the image |
| A9 | Translation attack |

watermark which is the measure of similarity between images. In the case of fragile watermarking, the NC value between the watermark and extracted image should be very low even after minimal modification to the watermarked image, serving the purpose of privacy and security. As the proposed method employs zero watermarking, there is no actual embedding in the cover image, and thus no metric is required to compare the watermarked and cover images as they are the same.

In order to extract feature maps from the cover image, diverse deep learning (DL) models were computed and executed on standard images in the face of attacks. These outcomes were then meticulously analyzed, and the average results are elucidated in table 6.

Table 6. Average NC after performing attacks on various DL architectures

| DL Tech. | A1 | A2 | A3 | A4 | A5 | A6 | A7 | A8 | A9 |
|-----------------|---------|---------|---------|---------|---------|---------|---------|---------|---------|
| $\mathbf{R50}$ | 0.0159 | -0.0175 | 0.0078 | -0.0054 | -0.0275 | -0.0435 | 0.0103 | -0.0068 | -0.0005 |
| $\mathbf{R101}$ | -0.0146 | 0.0008 | -0.0088 | 0.0056 | -0.0010 | -0.0039 | -0.0021 | -0.0076 | -0.0056 |
| VGG19 | 0.0070 | 0.0024 | -0.0167 | -0.0177 | 0.0037 | 0.0243 | -0.0220 | -0.0062 | -0.0091 |
| DN121 | 0.0071 | -0.0021 | -0.0087 | -0.0102 | -0.0142 | 0.0010 | 0.0036 | 0.0010 | -0.0138 |
| \mathbf{MNet} | 0.0200 | 0.0295 | -0.0039 | -0.0024 | -0.0191 | -0.0044 | -0.0079 | -0.0130 | 0.0090 |

Subsequent to running ResNet50, ResNet101, VGG19, DenseNet121, and MobileNet models, the deduction drawn from the results was that ResNet50 provided the most exceptional outcomes since it generated the minimum value of NC is majority of attacks and is giving best results from all other methods.

Furthermore, we also determined the average value of NC using ResNet50, by testing it on a medical image dataset against various attacks. The outcomes of ResNet 50 against various attacks on individual standard images and medical image dataset are tabulated in table 7. Hence the NC values obtained from the results are very low, this directly prove that the proposed method is highly tamper proof.

Table 7. Results of ResNet50

| Images | A1 | A2 | A3 | A4 | A5 | A6 | A7 | A8 | A9 |
|--------|---------|----------|---------|----------|---------|---------|----------|----------|---------|
| I1 | 0.0893 | -0.1022 | -0.0673 | 0.0288 | -0.0300 | -0.0306 | 0.0006 | -0.0187 | 0.0307 |
| I2 | 0.0726 | -0.0253 | 0.0685 | -0.0287 | 0.0131 | -0.0823 | -0.0091 | -0.0118 | -0.0486 |
| I3 | -0.0527 | 0.0047 | 0.0454 | 0.0252 | -0.0053 | -0.0465 | 0.0373 | -0.0172 | -0.0717 |
| I4 | -0.0860 | -0.1110 | 0.0264 | -0.0617 | -0.0043 | -0.0212 | -0.0277 | -0.0446 | 0.0010 |
| I5 | -0.0370 | 0.1179 | 0.0020 | -0.0136 | 0.0108 | -0.0347 | -0.0195 | -0.0602 | -0.0190 |
| I6 | 0.0347 | -0.0230 | 0.0068 | -0.0541 | -0.0058 | -0.0195 | 0.0786 | 0.0497 | -0.0157 |
| I7 | 0.0332 | -0.0556 | -0.0425 | -0.0198 | -0.0251 | -0.0956 | 0.0512 | -0.0076 | 0.0545 |
| I8 | 0.0262 | -0.0224 | -0.0531 | 0.0029 | -0.0726 | -0.0383 | 0.0339 | -0.0449 | -0.0112 |
| I9 | 0.0913 | -0.0205 | 0.0154 | 0.0037 | -0.0476 | -0.0559 | 0.0177 | 0.0131 | -0.0158 |
| I10 | 0.0094 | 0.0779 | 0.0037 | 0.0200 | -0.0669 | -0.0405 | -0.0163 | 0.0131 | 0.0269 |
| I11 | -0.0060 | -0.0325 | 0.0807 | 0.0376 | -0.0692 | -0.0134 | -0.0337 | 0.0544 | 0.0636 |
| I12 | 0.00005 | -0.00366 | 0.00492 | -0.00118 | 0.00036 | 0.00490 | -0.00352 | -0.00609 | 0.00124 |

5 Conclusion

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In conclusion, the security of digital images with sensitive and confidential data is of paramount importance to avoid severe penalties associated with unauthorized access. The proposed method in this manuscript is a highly effective solution to this problem. This technique initially employs NSST-DTCWT based multimodality image fusion method to generate the final watermark. By utilizing the avalanche effect of the hashing algorithm SHA512, the method is highly fragile. Any slight changes in the watermarked image can completely destroy the confidential information stored as the watermark image, effectively preventing any unauthorized access. Further, the implementation of virtual embedding with zero watermarking instead of actual embedding significantly reduces the attack surface as it conceals the availability of the watermark image in the cover image. This approach provides an additional layer of security by making it more difficult for attackers to identify and tamper with the watermark image. Therefore, this method provides an excellent solution to ensure the security of digital images with confidential information.

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